DOI: 10.7860/JCDR/2023/63343.17944 Original Article



Evaluation and Comparison of Momentto-Force Ratio of a New "PRP Loop" with that of Opus Loop and L Loop-A Finite Element Method Study

SMITA KUMARI¹, PRIYANKA NIRANJANE², PALLAVI DAIGAVANE³, RANJIT KAMBLE⁴



ABSTRACT

Introduction: Extraction space closure is the foremost challenging procedure in the field of orthodontics which needs a robust understanding of biomechanics. There are two commonly used methods of space closure, one which involves friction, also called sliding mechanics, and the other is frictionless. The advantages of frictionless mechanics are there is no force loss due to friction and low anchorage taxing. The preferred method for the retraction of teeth is loop mechanics and which ensures controlled tooth movement.

Aim: To evaluate and compare the Moment-to-Force (M/F) ratio of PRP loop with that of Opus loop and L loop by Finite Element Method (FEM).

Materials and Methods: An in-vitro study was conducted by using FEM analysis in DMIHER University with technical assistance from the Department of Mechanical Engineering VNIT Nagpur. Computer models of Loops design were prepared on Analysis of Systems (ANSYS) version 10 (V10) software. Opus loop, L loop and Platelet-Rich Plasma (PRP) loop were modelled as SOLID 64 beam elements. Different pre-activation

bends were given to the models in α and β nodes of the loop. Statistical analysis was done with Statistical Package for Social Sciences (SPSS) version 27.0 software to compare the mean of all three loops.

Results: Total 36 FEM models were studied. PRP loop showed greater M/F ratio than Opus and L loop with $15^{\circ}\alpha$ and $25^{\circ}\beta$ pre-activation bends in both 0.017×0.025 and 0.019×0.025 -inch Titanium Molybdenum Alloy (TMA) wire i.e., 9.09 and 9.12, respectively. On comparison of M/F ratio of PRP loop, Opus loop and L loop prepared with 0.017×0.025 and 0.019×0.025 TMA wire, at $15^{\circ}\alpha$ and $25^{\circ}\beta$ pre-activation bend in 0.019×0.025 TMA, PRP loop showed highest M/F ratio of 9.12 as compared to 0.017×0.025 TMA wire.

Conclusion: The study concluded that PRP loop is an efficient retraction loop with ideal moment force ratio for translatory movement of tooth. PRP loops had highest M/F ratio than Opus loop and L loop, indicating that PRP can be used for translatory movement of tooth in wires of different materials. Therefore, for proper utilisation of PRP loop, it must be prepared with either 0.017×0.025 inch TMA or 0.019×0.025 inch TMA wire.

Keywords: Finite element analysis, Friction mechanics, Loop mechanics, Retraction force

INTRODUCTION

Closure of the extraction space is the most challenging procedure in Orthodontics [1]. The skill required to close spaces, especially those caused due to extraction of teeth, is highly desired during the treatment. The two methods of space closure are sliding or friction mechanics and the other is frictionless or loop mechanics [2,3]. In sliding mechanics, friction is produced between the bracket and archwire when teeth slide along the base archwire. The disadvantages are that, the force magnitude cannot be readily determined and friction slows the movement of the teeth along the archwire [4].

In frictionless mechanics, loops and springs are preferred for the retraction of teeth, which ensures controlled tooth movement. Statistically quantified force is produced with an archwire which is under the operator's control. The advantage of the non-frictional approach is that there is no force loss due to friction and low anchorage taxing [5].

An ideal loop used for space closure should possess certain desirable characteristics like: i) a high moment-force ratio for translatory tooth movement; ii) a smaller Force-Deflection (F/D) rate for maintaining the ideal force system; iii) a large range of activation; iv) perfect size for fitting into the vestibule; and v) should be comfortable to the patient [6-9]. Different types of loops are used in space closure e.g., Opus loop, mushroom loop, L loop, vertical loop, T loop, teardrop loop, omega loop, K SIR loop, etc. A loop used for space closure must have a high M/F ratio i.e., closes to 10:1, and a low force-to-deflection rate [4].

To make the retraction loop invariably acceptable, a thorough understanding of its biomechanical properties is required. A blend of Opus loop and L loop was introduced by Dr Pallavi Daigavane in the Department of Orthodontics and Dentofacial Orthopaedics, Sharad Pawar Dental College, in the form of PRP loop [2]. PRP loop is an open loop and its design is similar to that of Opus loop and T loop. The M/F ratio of PRP loop has not been analysed. This study was therefore conducted to determine the M:F ratio of a new loop called PRP loop and compare it with Opus loop and T loop. FEM was used for this study in which, a 3-dimensional model of all three loops was generated and moment force ratio generated by loop geometries in 3-dimensional spaces was studied. The research protocol of this study has already been published [2].

MATERIALS AND METHODS

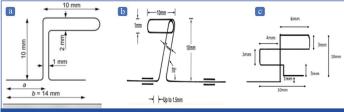
A cross-sectional study was conducted from 1st July 2022 to 1st December 2022. The study was carried out after approval from the Ethical Committee of Datta Meghe Institute of Higher Education & Research (DMIHER), Wardha, Maharashtra, India. (Ref.no. DMIMS(DU)/IEC/2020-21/9399 Dated 24/12/2020).

Loop models were fabricated in 0.017×0.025 -inch and 0.019×0.025 -inch wire dimensions in TMA wires [2]. Loop mechanics favour full slot engagement between the wire and bracket interface to prevent loss of torque during retraction. In 0.022-inch slot, 0.019×0.025 -inch wire was preferred and in 0.018-inch slot, 0.017×0.025 -inch wire was preferred [2].

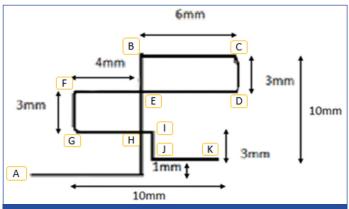
Procedure

Methodology: The initial modelling was done using Ansys workbench 16 software. The finite element analysis was done using ANSYS as the pre and post-processor and Ansys Direct solver was loaded on the International Business Management (IBM). Dimensions of the loop models were based on the prescription given by their respective authors. L loop was first described by Stoner MM in 1960 [10]. Opus loop was described by Siatkowski RE in 1977 [11]. A total of 36 finite element models were constructed for the study. The horizontal length of all the loop models (distance between the anterior and the posterior node) were kept 13 mm considering the inter-bracket distance from the second premolar mid-point to the canine mid-point.

L loop- Occluso-gingivally height was kept 10 mm and Mesiodistally it extended to 10 mm [2,10]. Opus loop- Occluso-gingivally height was kept 10 mm and mesiodistally it extended to 10 mm [2,11]. PRP loop was designed by Dr. Pallavi Daigavane. Dimension-Occluso-gingivally height was kept 10 mm and mesio-distally extended to 10 mm [Table/Fig-1a-c] [2]. The loop was called PRP based on its structure which resembles the three alphabets P, R, and P. When the clinicians start fabricating the loop, they bend the wire in the shape of P then further extend the wire and make the reverse P. After that, the clinicians end this structure by bending the wire in the shape of R [Table/Fig-2].



[Table/Fig-1]: Figures of (a) L loop; (b) Opus loop; (c) PRP loop.

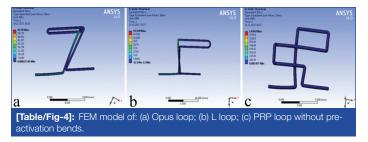


[Table/Fig-2]: Explanation of the structure defining the name PRP loop. 1) Starting with A, the authors make the first loop as A, H, E, B, C, D, E as first P. 2) Extending E, to make second P loop as D, E, F, G, H (reverse P). 3) Extending point H to form R shape as H, I, J, K.

Different pre-activation bends were given in all three loops on alpha side (towards canine bracket) and beta side (towards premolar bracket) and models were prepared accordingly. Thirty-six loop models were prepared with and without pre-activation bends for the study [Table/Fig-3,4].

0.017×0.025 and 0.019×0.025 TMA wire						
PRP Loop	L Loop	Opus Loop				
0° α and 0° β	0° α and 0° β	0° α and 0° β				
0° α and 25° β	0° α and 25° β	0° α and 25° β				
0° α and 35° β	0° α and 35° β	0° α and 35° β				
10° α and 45° β	10° α and 45° β	10° α and 45° β				
15° α and 25° β	15° α and 25° β	15° α and 25° β				
30° α and 0° β	30° α and 0° β	30° α and 0° β				

[Table/Fig-3]: Loop models of PRP loop, L loop and Opus loop.



Methodology for analysis:

- For loops without pre-activation bends: After modelling of the loops, a fixed point was determined on the alpha position (towards the canine bracket). The terminal node on the beta side (towards premolar bracket) was displaced by 1 mm. Force and moment was produced on the terminal node towards the alpha side (towards canine bracket).
- ii. For loops with pre-activation bends:

Methodology for analysis of loops with pre-activation bends:

Step 1: Loops were prepared with pre-activated bends and imported to ANSYS for analysis [Table/Fig-4a-c].

Step 2: The terminal β node towards premolar was fixed and α segment towards canine was displaced.

Step 3: Displacement was given between 0.1-1 mm. At each displacement moment and force were noted on terminal nodes.

Step 4: Subsequently, the terminal node on the beta side towards premolar bracket was displaced by 1 mm, after which the force and the moment produced on the terminal node was recorded.

STATISTICAL ANALYSIS

The statistical analysis was carried out using IBM SPSS version 27.0 software. To compare the performance of three loops (PRP Loop, Opus Loop, and L Loop), the one-way Analysis of Variance (ANOVA) test and group descriptive function of the software was utilised to compare the means and to find out group descriptive. According to the analysis, the moment force ratio of the PRP loop was maximum with a minimum standard deviation of 0.45 as compared to the other two loops, and moment force ratio of L loop was minimum, with a maximum standard deviation of 0.78.

RESULTS

Total 36 FEM models were studied to evaluate the M/F ratio, and the maximum force generated by the respective Loop Models after their activation. Statistical analysis showed that the M/F ratio mean at different pre-activation bends of PRP loop was 8.37, Opus loop was 6.37 and L loop was 5.27. Therefore, according to [Table/Fig-5,6] PRP had the highest value of M/F ratio mean in comparison of other two loops.

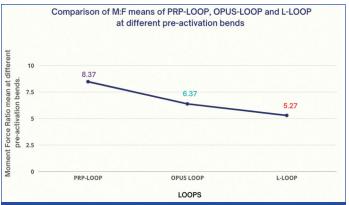
Type		Mean		Stan-	95% confidence interval for mean				
of loop	of M/F		Standard Deviation	dard Error	lower bound	upper bound	Minimum	Maximum	
PRP Loop	6	8.47	0.45	0.18	8.0	8.94	7.77	9.09	
OPUS Loop	6	6.37	0.60	0.24	5.73	7.00	5.36	7	
L Loop	6	5.26	0.78	0.32	4.44	6.09	4.63	6.72	

[Table/Fig-5]: Means of M/F ratio of PRP: Platelet-Rich Plasma loop, Opus loop, and L loop.

In 0.017×0.025 TMA wire without pre-activation bend at $0^{\circ}\alpha$ and $0^{\circ}\beta$ bend with displacement of 0.1 to 1 mm; M/F ratio of PRP loop was 8.30, Opus loop was 6.84 and L loop was 5.60. PRP loop showed greater M/F ratio than Opus and L loop with 0° pre-activation bends [Table/Fig-7,8]. After increasing pre-activation bend with displacement of 0.1 to 1 mm; PRP loop had higher M/F

ratio than Opus and L loop. At pre-activation bend of $15^{\circ}\alpha$ and $25^{\circ}\beta$ bend; PRP loop showed highest M/F ratio of 9.09 whereas Opus loop showed 6.55 and L loop showed 4.85. This indicated that at $15^{\circ}\alpha$ and $25^{\circ}\beta$ bend, PRP loop had more bodily or translatory movement as compared to Opus loop and L loop [Table/Fig-7,8].

In 0.019×.025 TMA wire without pre-activation bend at $0^{\circ}\alpha$ and $0^{\circ}\beta$ bend with displacement of 0.1 to 1 mm; M/F ratio of PRP loop was 8.30, Opus loop was 6.84 and L loop was 5.60. PRP loop showed greater M/F ratio than Opus and L loop with 0° pre-activation bends [Table/Fig-9,10]. After increasing pre-activation bend with displacement of 0.1 to 1 mm; PRP loop had higher M/F ratio than Opus and L loop. At pre activation bend of $15^{\circ}\alpha$ and $25^{\circ}\beta$ bend PRP loop showed highest M/F ratio of 9.12 whereas Opus loop



[Table/Fig-6]: Graphical representation of a comparison of M/F means of PRP loop, Opus loop and L-loop at different pre-activation bends.

showed 6.61 and L loop showed 5.04. This indicated that at $15^{\circ}\alpha$ and $25^{\circ}\beta$ bend, PRP loop had more bodily or translatory movement [Table/Fig-9,10].

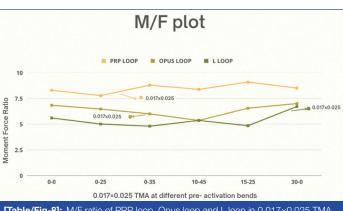
On comparison of M/F ratio of all three loops prepared with 0.017×0.025 and 0.019×0.025 TMA wire without pre-activation bend M/F ratio of PRP loop was 8.30, Opus loop was 6.84 and L loop was 5.60. PRP loop had highest M/F ratio than Opus and L loop [Table/Fig-11]. At $15^{\circ}\alpha$ and $25^{\circ}\beta$ pre-activation bend in 0.019×0.025 TMA, PRP loop showed highest M/F ratio of 9.12 as compared to 0.017×0.025 TMA wire. [Table/Fig-11,12].

DISCUSSION

The result showed that the inherent M/F ratio produced by PRP loop prepared in TMA wire with dimensions 0.019×0.025-inch and 0.017×0.025-inch without pre-activation bend that is 0° α and β bend is not adequate to impart translatory movement of the dentition. To increase the M/F ratio close to 8-10, gable pre-activation bends were given. PRP loop models prepared in TMA wire with 0.017×0.025-inch and 0.019×0.025-inch dimension needs a pre-activation bend to produce an ideal M/F ratio in the range of 8-10 which is very important for translatory movement of the dentition.

M/F ratio for all the PRP loop models was in the range of 7-10 in the present study. This is an important characteristic of any retraction loop. M/F ratio of any retraction loop is closely related to the centre of rotation of the dentition. As the M/F ratio changes, accordingly the centre of rotation will change and this will cause inconsistent distribution of stress along the periodontium which is not ideal condition during the process of space closures [7].

0.017×0.025	PRP Loop				OPUS Loop		L Loop			
TMA	Force (N)	Moment (N-mm)	M:F	Force	Moment	M:F	Force	Moment	M:F	
0-0	0.428	3.554	8.30	0.01	1.35	6.84	0.15	0.85	5.60	
0-25	1.396	10.86	7.77	0.14	0.94	6.47	0.20	1.01	5.01	
0-35	1.02	8.78	8.79	0.14	0.87	6.0	0.21	1.03	4.80	
10-45	1.77	14.92	8.38	0.15	0.81	5.36	0.22	1.04	4.63	
15-25	1.18	10.78	9.09	0.14	0.95	6.55	0.20	0.98	4.85	
30-0	1.03	8.77	8.51	0.19	1.37	7.0	4.47	30.10	6.72	



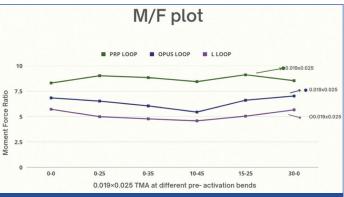
[Table/Fig-8]: M/F ratio of PRP loop, Opus loop and L loop in 0.017×0.025 TMA at different pre-activation bends.

In the present study, L loop with 0.017×0.025 TMA and 0.019×0.025 TMA wire showed M/F ratio of 5.60 at 0° preactivation bend which was similar to a study conducted by Safavi MR et al., [12]. The author compared four different loops that is T loop, L loop, Opus loop and vertical helical, closing loop prepared with 0.016×0.022 SS wire with different pre-activation bends with the help of FEM study and found that M/F ratio of L loop was 4.6 at 0° pre-activation bend and for Opus loop were 7.6 at 1 mm displacement. The reading for Opus loop obtained in the present study at 1 mm displacement was 6.84. This variation might be because of difference in wire material or dimension of wire. TMA wire is more resilient and less stiff than stainless steel wire. TMA produces less force for a longer duration whereas stainless steel wire produces more force for shorter duration.

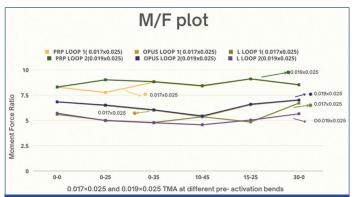
0.019×0.025	PRP loop			OPUS loop			L loop		
TMA	Force (N)	Moment (N-mm)	M:F	Force	Moment	M:F	Force	Moment	M:F
0-0	1.42	11.83	8.30	0.27	1.85	6.84	0.015	0.08	5.60
0-25	1.62	14.69	9.02	0.20	1.309	6.52	0.28	1.40	4.99
0-35	1.91	16.96	8.84	0.19	1.2	6.05	0.30	1.43	4.77
10-45	2.439	20.609	8.44	0.20	1.13	5.44	8.55	39.22	4.58
15-25	1.638	14.955	9.12	0.20	1.32	6.61	7.84	39.52	5.04
30-0	1.432	12.221	8.53	0.27	1.92	7.03	5.95	33.75	5.66

[Table/Fig-9]: M/F ratio of PRP loop, Opus loop and L loop in 0.019×0.025 TMA at different pre-activation bends

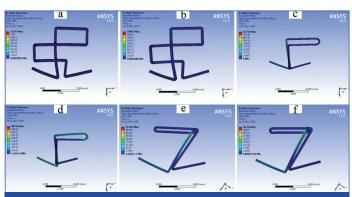
[Table/Fig-7]: M/F ratio of PRP loop, Opus loop and L loop in 0.017×0.025. TMA at different pre-activation bends.



[Table/Fig-10]: M/F ratio of PRP loop, Opus loop and L loop in 0.019×0.025 TMA at different pre-activation bends.



[Table/Fig-11]: M/F ratio of PRP loop, Opus loop and L loop in 0.017×0.025 and 0.019×0.025 TMA at different pre-activation bends.



[Table/Fig-12]: FEM models of: (a) 0.017×0.025 TMA PRP loop at $15^{\circ}\alpha$ and $25^{\circ}\beta$ pre activation bend; (b) 0.019×0.025 TMA PRP loop at $15^{\circ}\alpha$ and $25^{\circ}\beta$ preactivation bend; (c) 0.017×0.025 TMA L loop at $15^{\circ}\alpha$ and $25^{\circ}\beta$ pre-activation bend; (d) 0.019×0.025 TMA L loop at $15^{\circ}\alpha$ and $25^{\circ}\beta$ pre-activation bend; (e) 0.017×0.025 TMA Opus loop at $15^{\circ}\alpha$ and $25^{\circ}\beta$ pre-activation bend; (f) 0.019×0.025 TMA Opus loop at $15^{\circ}\alpha$ and $25^{\circ}\beta$ pre-activation bend.

The M/F ratio of TMA is higher than stainless steel indicating that TMA is able to produce more bodily or translatory movement than stainless steel [12].

In the present study, the M/F ratio of Opus loop was between 5-7 in 0.017×0.025-inch and 0.019×0.025-inch TMA wire. The M/F ratio of Opus loop was between 8.5-9.3 at 0-degree pre-activation with displacement of 0-2 mm reported by Techalertpaisarn P and Versluis A, in his study [13]. The authors compared the opus loop with T loop and L loop fabricated in a 0.016×0.022-inch stainless steel wire. Opus loops and L-loops showed the highest M/F ratio (8.5-9.3) on the canine bracket when the loop was centred. The difference of M/F ratio between both studies might be because of different wire material or different softwares used for FEM study.

The M/F ratio of L loop was in the range of 4-6 in the present study which was similar to study conducted by Cai Y [14]. The author evaluated and compared M/F ratio of vertical, L and T-loop in both TMA and stainless-steel arch wire and concluded that TMA generated M/F ratio of vertical loop was 3.235 mm, L loop was 4.768 mm, and T loop was 6.95.

There is less research about properties of L loop, but according to Savafi MR et al., Siatkowski RE; this loop had higher values of force and moment, without angular bend [11,12]. When angular bend was given, moment, force, and M/F of the L loop decreased similar to other loops, but by enhancing activation range, its moment increased greater than other loops. According to Burstone CJ and Koenig HA; Faulkner MG et al., Menghi C et al., Chen J et al., Thiesen G et al., increasing the wire length and adding a helix can cause reduction in force [6,15-18].

In our study, M/F ratio of Opus loop was 6.84 at 0° pre-activation bend. A similar FEM study conducted by Rao PR et al., to evaluate and compare snail loop with Opus loop and tear drop loop. He found that at 0° pre-activation bend M/F ratio of Opus loop was 9.8 in 0.019×0.025-inch TMA wire [19]. This difference might be because of difference in software used in FEM study [19].

Thus, after evaluating and comparing M/F ratio of Opus loop, L loop and PRP loop, the authors can say that PRP loop has a definite advantage over L loop in all respects of M/F ratio. Even in comparison to Opus loop, PRP loop has a distinct advantage that with incorporation of gable bends, PRP loop is very efficient to deliver M/F ratio in an ideal range, PRP loop has a better shape morphology as compared to Opus loop which prevents any problem of tissue impingement and also fabrication time of PRP loop is very less as compared to Opus loop.

Limitation(s)

The study only evaluated M/F ratio. F/D rate can also be evaluated before clinical application of the PRP loop.

CONCLUSION(S)

After evaluating the M/F ratio of PRP loop, Opus loop and L loop, it can be concluded that PRP loop is an efficient retraction loop with ideal M/F ratio for translatory movement of tooth. PRP loop, Opus loop and L loop showed insufficient M/F ratio without preactivation bend. As the pre-activation bend increased, M/F ratio also increased in both 0.017×0.025 inch and 0.019×0.025-inch TMA wires. PRP loops had highest M/F ratio than Opus loop and L loop, indicating that PRP can be used for translatory movement of tooth in both wires. On comparing 0.017×0.025 inch and 0.019×0.025 inch PRP loop, 0.019×0.025 inch TMA wire had more M/F ratio. Further clinical trials are recommended for frictionless closure of extraction space. Results obtained must be further substantiated by experimental investigation and clinical study. The study evaluated M/F ratio, F/D rate can also be evaluated before clinical application of the PRP loop.

REFERENCES

- [1] Braun S, Sjursen RC, Legan HL. On the management of extraction sites. Am J Orthod Dentofacial Orthop. 1997;112(6):645-55.
- [2] Kamble R, Niranjane P, Kumari S. Evaluation and comparison of biomechanical properties of a new "PRP Loop" with that of Opus Loop and L-Loop-a FEM study. Journal of Pharmaceutical Research International. 2021;33(64A):75-79.
- [3] Staggers JA, Germane N, Legan HL. Clinical considerations in the use of protraction headgear. J Clin Orthod. 1992;26(2):87-91. PMID: 1430168.
- [4] Choy K, Pae EK, Kim KH, Park YC, Burstone CJ. Controlled Space Closure with a Statically Determinate Retraction System. Angle Orthod. 2002;72(3):191-98.
- [5] Rhee JN, Chun YS, Row J. A comparison between friction and frictionless mechanics with a new typodont simulation system. Am J Orthod Dentofacial Orthop. 2001;119(3):292-99.
- [6] Burstone CJ, Koenig HA. Optimizing anterior and canine retraction. Am J Orthod. 1976;70(1):01-19.
- 7] Tanne K, Koenig HA, Burstone CJ. Moment to force ratios and the center of rotation. Am J Orthod Dentofacial Orthop. 1988;94(5):426-31.
- [8] Burstone C. Modern Edgewise Mechanics. 2nd edition, Mosby publications Ltd.;1995(cited 2022 Nov 26):04-05.
- [9] Rinaldi TC, Johnson BE. An analytical evaluation of a new spring design for segmented space closure. Angle Orthod. 1995;65(3):187-98.
- [10] Stoner MM. Force control in clinical practice: I. An analysis of forces currently used in orthodontic practice and a description of new methods of contouring loops to obtain effective control in all three planes of space. American Journal of Orthodontics. 1960:46(3):163-86.

- [11] Siatkowski RE. Continuous arch wire closing loop design, optimization, and verification. Part H. Am J Orthod Dentofacial Orthop. 1997;112(4):393-402.
- Safavi MR, Geramy A, Khezri AK. M/F ratios of four different closing loops: 3D analysis using the finite element method (FEM). Aust Orthod J. 2006;22(2):121-26.
- [13] Techalertpaisarn P, Versluis A. T-loop force system with and without vertical step using finite element analysis. Angle Orthod. 2016;86(3):372-79.
- [14] Cai Y. Finite element analysis of archwire parameters and activation forces on the M/F ratio of vertical, L- and T-loops. BMC Oral Health. 2020;20(1):70.
- Faulkner MG, Lipsett AW, El-Rayes K, Haberstock DL. On the use of vertical loops in retraction systems. Am J Orthod Dentofacial Orthop. 1991;99(4):328-36.
- [16] Menghi C, Planert J, Melsen B. 3-D experimental identification of force systems from orthodontic loops activated for first order corrections. The Angle Orthodontist. 1999;69(1):49-57.
- Chen J, Markham DL, Katona TR. Effects of T-loop geometry on its forces and moments. The Angle Orthodontist. 2000;70(1):48-51.
- Thiesen G, do Rego MV, de Menezes LM, Shimizu RH. Force systems yielded by different designs of T-loop. Aust Orthod J. 2005;21(2):103-10. PMID: 16429865.
- [19] Rao PR, Shrivastav SS, Joshi RA. Evaluation and comparison of biomechanical properties of snail loop with that of opus loop and teardrop loop for en masse retraction of anterior teeth: FEM study. J Ind Orthod Soc 2013;47(2):62-67.

PARTICULARS OF CONTRIBUTORS:

- Student (Postgraduate), Department of Orthodontics and Dentofacial Orthopedics, Sharad Pawar Dental College, Wardha, Maharashtra, India.
- Reader, Department of Orthodontics and Dentofacial Orthopedics, Sharad Pawar Dental College, Wardha, Maharashtra, India.
- 3.
- Reader, Department of Orthodontics and Dentofacial Orthopedics, Sharad Pawar Dental College, Wardha, Maharashtra, India.

 Professor and Head, Department of Orthodontics and Dentofacial Orthopedics, Sharad Pawar Dental College, Wardha, Maharashtra, India.

NAME, ADDRESS, E-MAIL ID OF THE CORRESPONDING AUTHOR:

Smita Kumari.

Student (Postgraduate), Department of Orthodontics and Dentofacial Orthopedics, Sharad Pawar Dental College, Wardha, Maharashtra, India. E-mail: smita3345@gmail.com

AUTHOR DECLARATION:

- Financial or Other Competing Interests: None
- Was Ethics Committee Approval obtained for this study? Yes
- Was informed consent obtained from the subjects involved in the study? NA
- For any images presented appropriate consent has been obtained from the subjects. NA

PLAGIARISM CHECKING METHODS: [Jain H et al.]

ETYMOLOGY: Author Origin

• Plagiarism X-checker: Feb 09, 2023

• Manual Googling: Apr 07, 2023

• iThenticate Software: Apr 20, 2023 (16%)

Date of Submission: Feb 08, 2023 Date of Peer Review: Feb 28, 20223 Date of Acceptance: Apr 24, 2023 Date of Publishing: May 01, 2023